

**AMENDMENTS TO THE SPECIFICATION**

Please amend the title on page 1 as follows:

AN IMAGING SYSTEM INCLUDING IMPROVED DESIGN AND MANUFACTURING  
APPROACH TO THE IMPLEMENTATION OF A MICROLENS-ARRAY BASED  
SCINTILLATION CONVERSION SCREEN

Please amend the first paragraph of the specification under the heading CROSS-REFERENCE  
TO RELATED APPLICATIONS, (on page 1) as follows:

This application is a divisional application of Serial No. 10/118,368, which is a divisional  
application of Serial No. 09/740,148, filed December 18, 2000 now U.S. Patent No. 6,389,105,  
which is a continuation-in-part of application Serial No. 09/225,885, filed January 5, 1999, now  
U.S. Patent No. 6,178,224, which is a continuation-in-part of application Serial No. 09/076,604,  
filed May 11, 1998, now U.S. Patent No. 5,909,478, which is a divisional application of Serial  
No. 08/773,483, filed 12/23/96 December 23, 1996, now U.S. Patent No. 5,828,726, which is a  
continuation of application Serial No. 08/494,251, filed June 23, 1995 06/23/95, now U.S. Patent  
No. 5,608,774. U.S. Patent No. 6,205,199, is also referenced.

Please amend the paragraph beginning on page 18, line 33 and ending on page 19, line 4 as  
follows:

“In order to reduce the number of X-rays that strike the camera 48, the camera 48 is  
encased in a 0.125 inch thick lead housing or shield 50. The preferred shield 50, for use with the  
particular CCD camera 48 specified above, is shown in its folded state in FIG. 5, before placing  
it around the CCD camera 48. In addition, a 0.25 inch thick lead plate ~~52~~51 may be placed

between the CCD-chip and incident X-ray radiation in order to further shield the CCD chip from stray X-rays.”

Please amend the paragraph after the header "ABSTRACT" on page 49 as follows:

A portable, self-contained, electronic radiosopic imaging system ~~uses a pulsed X-ray source, a remote X-ray sensor, and a self-contained, display and controller unit to produce, store, and/or display digital radiosopic images of an object under investigation in low voltage imaging environments such as medical applications including mammography and tissue imaging, and industrial radiography of low density structures, or the like. The radiographic system uses an X-ray converter screen for converting impinging X-ray radiation to visible light, and thus each point impinged on the screen by X-ray radiation scintillates visible light emissions diverging from the screen. An image sensor, i.e., a CCD camera, is configured to sense the visible light from the screen. An aspheric objective lens operable with the CCD camera spatially senses visible light within a collection cone directed outwardly from the image sensor. An emission modification lens layer, e.g., a prismatic brightness enhancement film or a sprayed on transmissive layer, through which the visible light emitted from the screen is transmitted is superposed with the screen and positioned in an optical path between the aspheric lens and the screen for generally focusing the diverging visible light as a restricted cone of illumination propagating outwardly from each point impinged on the screen to increase the fraction of light directed into the collection cone of the first lens and reducing the amount of scattered visible light from the screen.~~

**AMENDMENTS TO THE DRAWINGS**

In the attached drawings, the following changes have been made:

FIG. 3A – the reference numeral “52” has been changed to –51--;

FIG. 3B – the legend “PRIOR ART” has been added.